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Subcellular Control over Focal Adhesion Anisotropy, Independent of Cell Morphology, Dictates Stem Cell Fate

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Supporting Information

ABSTRACT: Although microscale patterning techniques have been used to control cell morphology and shape, they only provide indirect control over the formation of the subcellular cytoskeletal elements that determine contractility. This paper addresses the hypotheses that nanoscale anisotropic features of a patterned matrix can direct the alignment of internal cytoskeletal actin fibers within a confined shape with an unbiased aspect ratio, and that this enhanced control over cytoskeletal architecture directs programmed cell behaviors. Here, large-area polymer pen lithography is used to pattern substrates with nanoscale extracellular matrix protein features and to identify cues that can be used to direct cytoskeletal organization in human mesenchymal stem cells. This nanopattern-



ing approach is used to identify how anisotropic focal adhesions around the periphery of symmetric patterns yield an organized and contractile actin cytoskeleton. This work reports the important finding that anisotropic cues that increase cell contractility within a circular shape redirect cell differentiation from an adipogenic to an osteogenic fate. Together, these experiments introduce a programmable approach for using subcellular spatial cues to control cell behavior within defined geometries.

KEYWORDS: cell adhesion, nanopatterning, polymer pen lithography, image analysis, cytoskeleton, actin

he organization of the extracellular matrix (ECM) at both nano and micro length scales directs the formation of focal adhesion (FA) complexes in adherent cells and, in turn, influences cytoskeletal organization, cell shape, and specific cellular responses such as migration, survival, and differentiation.¹⁻³ The development of methods that can pattern protein ligands on solid substrates has been important for controlling cell adhesion⁴⁻¹³ and understanding the many ways in which cells respond to ECM organization at a range of length scales.^{4,14-20} Importantly, the use of approaches to pattern adhesive cues has provided significant insight into more complex behaviors including migration,^{21,22} differentiation,^{23–27} survival,^{25,28,29} and signaling.^{13,30,31} Significant work has used microcontact printing to demonstrate how global cell shape directs the formation of focal adhesions at local regions of the cell perimeter.^{31–33} It is also commonly observed that FAs adopt an elongated morphology at the edges of the cell, with an alignment that corresponds with that of the associated actin stress filaments. Aligned and elongated focal adhesions are also observed in cells cultured on unpatterned substrates, where cell spreading is not restricted to a predefined geometry. This observation raises the question of whether ECM ligands that are patterned into subcellular asymmetric

features can, in turn, direct the organization of the cytoskeleton, with downstream effects on cell behaviors.

A series of landmark studies have demonstrated how substrates that are nanopatterned with ECM ligands can control cell adhesion and influence cell activities. Spatz and co-workers, for example, used micelle block copolymer lithography to show that a maximal distance of ~50–70 nm between individual integrin molecules can still support integrin clustering for effective cell adhesion and spreading, and that greater interligand spacing decreases cell function.⁵ Furthermore, nanostructured topographies presenting cell adhesion ligands can enhance osteogenic differentiation when moderate disorder is present, which supports the formation of stable focal adhesions.^{34,35} Other studies further reveal the exquisite sensing capability of cells to respond to nanoscale variations in the size, spacing, composition, and topology of patterned cues presented on substrates.^{3-6,8,30,36,37}

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Figure 1. Actin fiber orientation within cells on square substrates. (a-d) Pattern designs (left) and representative fluorescence micrographs of the actin cytoskeleton in hMSCs seeded on each pattern (right). (e) Fluorescence image of fibronectin patterned as a square dot matrix (left), representative fluorescence image of the actin cytoskeleton of a cell on a square dot matrix pattern (center), and heatmap of the average actin fiber staining intensity across a population of cells on the square dot matrix substrate (n = 78; right). (f) Fluorescence image of fibronectin patterned as an anisotropic square (left), representative fluorescence image of the actin cytoskeleton of a cell on an anisotropic square pattern (center), and heatmap of the average actin fiber staining intensity across populations of cells on the square substrate (n = 64; right). (g) Actin fiber orientation within cells on anisotropic and square dot matrix patterns (mean \pm SEM; **p < 0.01, ***p < 0.001, two-way ANOVA with Bonferroni *post hoc*).

Although previous studies have explored the influence of cellular-scale anisotropic patterns on cytoskeleton organization and cell behaviors,^{12,22,38-41} this work addresses the role of anisotropic nanoscale features on cytoskeletal organization within defined geometries (i.e., squares and circles). Studies have been limited in exploring the role of feature anisotropy in directing cell behavior, in large part because the patterning methods to control geometry at a submicron length scale have not been readily available. Indeed, most high-resolution nanopatterning techniques are labor-intensive, are timeconsuming, and provide limited throughput. Here, we use the emerging high-throughput, high-resolution, large-area nanopatterning technique, polymer pen lithography (PPL),⁴²⁻⁴⁵ to pattern submicron fibronectin features with aspect ratios of 4-6:1, and we show that the orientation of the fibronectin features can direct the alignment of the actin stress filaments in adherent cells.^{18,42,43,46,47} PPL can be used to define subcellular protein features with arbitrary size and shape over cm² areas, allowing one to probe many cells at once under nearly identical conditions, thereby providing a route to statistically meaningful data. Here, we use this technique to nanopattern fibronectin into predefined geometries and the subcellular arrangements to test the influence of anisotropy as a cue that directs the assembly of the cytoskeleton and downstream signaling. Significantly, we show that anisotropic focal adhesions provide control over the uniformity and directionality of the actin cytoskeleton. Whereas it has been

shown that the anisotropy of focal adhesions increases with increasing cell aspect ratios,⁴⁸ our use of PPL allows independent control over cell shape and anisotropic presentation of fibronectin and therefore can provide an understanding of how subcellular cues can independently direct assembly of the cytoskeleton with control over contractility and differentiation. Here, we show how this approach has identified two shape factors that enhance osteogenesis.

RESULTS AND DISCUSSION

Generating Arbitrary Patterns for Cell Adhesion and Differentiation Studies Using PPL. We used PPL to rapidly prepare substrates having nanoscale patterns of fibronectin with defined geometries. Pen arrays consisting of ~10 000 polymeric tips were inked with 16-mercaptohexadecanoic acid (MHA) and loaded into a PPL instrument. Patterns of MHA features were generated on gold-coated glass slides (Figure S1a). To validate that patterns were printed successfully, a portion of the gold-coated glass substrates was chemically etched, and the resulting MHA printed substrates were visualized with optical microscopy (Figure S1b). Next, the MHA patterned slides were treated with an ethanolic solution containing a hexa(ethylene glycol)-terminated alkanethiol, which backfilled the unmodified regions of gold with a chemically inert monolayer¹⁸ and which prevents the nonspecific protein adsorption in these experiments. Fibronectin



Figure 2. Actin fiber orientation within cells on circular substrate. (a) Fluorescence micrograph of fibronectin patterned in different circular shapes. (b) Representative fluorescence images of the actin cytoskeleton of cells seeded on each pattern. (c) Heatmap of the average actin fiber staining intensity across populations of cells on each circle pattern (n = 84), 20-point circles (n = 57), and hybrid circles (n = 46). (d) Angular distribution of radial fibers within the cells on all three circular patterns (mean \pm SEM). (e) Fast Fourier transform of the angular distribution of the radially oriented actin fibers (mean \pm SD).

was then introduced on the surfaces to allow it to adsorb to the MHA features (Figure S1a). Fluorescence micrographs confirm the discrete localization of antibody-labeled fibronectin on the surface in an arrangement defined by the MHA features (Figure S1c). This process was used to prepare a range of substrates having several arrangements of fibronectin features for subsequent studies of cytoskeletal organization in adherent cells.

Cell Cytoskeleton Organization on Square Geometries. In a first example, we printed an array of square features (54 \times 54 μ m²), each consisting of a dot matrix of 19 \times 19 square fibronectin features of approximately 750 nm dimension (Figure 1a,e). We cultured human mesenchymal stem cells (hMSCs) on a substrate that presents a uniform distribution of isotropic fibronectin features within the square geometry, which serves as a benchmark for identifying the influence of anisotropic fibronectin features. After 16 h of culture, we fixed and stained the actin cytoskeleton with a phalloidin-conjugated fluorophore and then imaged the hMSCs using confocal microscopy. We generated heatmaps by superimposing fluorescence micrographs of the actin cytoskeleton; these heatmaps confirmed that the square dot matrix pattern indeed does not induce any directional assembly of actin filaments (Figure 1e, right panel). The distribution of stress fibers, however, localizes along the periphery of the patterned square shape in most hMSCs.

Next, we prepared substrates that were patterned with asymmetric features to ask whether the orientation and aspect ratio of anisotropic features could control the cytoskeleton while maintaining constant cell size and shape. Specifically, we asked whether the direction of actin stress filaments would correspond to the orientation of the anisotropic focal adhesions. Hence, we designed and printed a set of patterns having (1) a center region presenting features arranged in a uniform square dot matrix that would provide sufficient ECM to support cell attachment and (2) a region along the periphery of the pattern where ligand arrangement and aspect ratio are varied (Figures 1b–d). Importantly, the overall shape of the pattern and feature density were approximately identical for the square patterns, and therefore, the cells attached to these patterns still maintained a 1:1 aspect ratio.

Fluorescence micrographs of actin fibers reveal that the anisotropic fibronectin features along the perimeter of the square shape could reinforce the alignment of actin fibers when they were aligned with the diagonal axes of the overall shape (Figure 1b). For cells seeded on the inverse anisotropic square patterns, where the fibronectin features are oriented perpendicular to the diagonal axis of the cell, actin fibers still

preferentially aligned diagonally across the cell (Figure 1c). In contrast, features arranged vertically around the periphery did not induce actin fibers to arrange along the edges of the pattern (Figure 1d). Instead, these cues disrupted the organization of the cytoskeleton observed in the parent pattern.

These results suggest that the cues associated with a square cell shape dominate over those associated with the nanoscale fibronectin features; the corners of square shapes, for example, have been shown to be sites for recruitment of focal adhesions and associated stress filaments. We find that cells on all three patterns having different orientations of the anisotropic fibronectin features share a similar organization of the cytoskeleton that is determined by the global cell shape and not the orientation of the anisotropic fibronectin features. However, we do find that the pattern having anisotropic fibronectin features aligned with the diagonal axis shows the most organized cytoskeleton (Figure 1b).

To quantitatively assess the role of anisotropic fibronectin feature orientation on actin organization, we performed an indepth analysis on these cells (Figure 1f). For this analysis, we compared the distribution of actin fibers in hMSCs on the square dot matrix pattern to those on the anisotropic square of the same size (Figure 1e,f). Heatmaps of the average actin fluorescence intensity show preferential alignment of fibers toward the interior of the cell on the square anisotropic pattern (Figure 1f, right panel). When we quantified fiber orientation using a gradient detection method,⁴⁹ the fiber alignment indeed increased along the long axes $(+45^{\circ} \text{ and } -45^{\circ})$ for cells on anisotropic patterns compared to the square dot matrix (Figure 1g). These results show that the anisotropic arrangement of adhesion ligands supports the assembly of userdirected actin architectures. In addition, when we increased the area of this pattern-where the center region of the dot matrix pattern was increased from 30×30 to $40 \times 40 \ \mu m^2$, we found that the anisotropic features had the same influence on cytoskeletal alignment (Figure S2).

MSC Cytoskeleton Organization on Circular Geometries. As described above, the strong global cues of the square patterns-which lead to stress filaments aligned along the diagonals of the cell-dominated over the anisotropic fibronectin features. Hence, we next repeated these experiments using circular patterns, which have been demonstrated to only weakly direct the assembly of the cytoskeleton.²³ In this way, we could determine whether the anisotropic features, absent global shape cues, could direct cytoskeletal assembly. We prepared patterns having a radius of 31 μ m because they would have the same area as the square patterns described above. Again, we generated a set of patterns to examine parameters that may affect actin fiber alignment (Figure S3ah). Previous studies have shown that circumferential and chordal fibers are the primary actin orientations within cells seeded on microcontact printed circular geometries.⁵⁰ Therefore, we varied the distribution of fibronectin in two ways: (1)concentric rings were introduced within the circle, and (2) periodic, anisotropic features consisting of anisotropic dot lines were placed around the periphery. In addition, all patterns contained a central region presenting fibronectin features arranged in a circular dot matrix that supports cell attachment and spreading.

Fluorescence micrographs confirmed the formation of circumferential and radial actin fibers within hMSCs on all the circular shapes (Figure S3a-h). However, circular shapes with concentric rings of fibronectin features did not

significantly change the circumferential fiber distribution within the cells (Figure S3b,d-f). On the other hand, when we introduced anisotropic features radially around the circle, actin fibers assembled in a periodic fashion, reflecting the pattern design (Figure S3g). We also note that a sparse spacing between peripheral features promotes different cell geometries that no longer reflect a circular shape (Figure S3h). From this library, we identified a periodic pattern consisting of 20 anisotropic features arranged around the cell periphery that promoted the formation of distinct radial fibers (Figure 2b,c).

We compared cells seeded on the 20-point circle to those seeded on patterns presenting symmetric features arranged in a circular shape (Figure 2a,b). Heatmaps of the average actin intensity reveal a periodicity in the radial fiber distribution within cells on 20-point circles that is not observed when cells are seeded on dot matrix circles (Figure 2c). In order to assess the periodicity of the fibers, the local fiber orientation was determined, and the fibers were classified as either radial or circumferential depending on the local orientation of the fiber relative to the centroid of the cell (Figure S4). The angular distribution of the radial fibers has a clear periodicity within cells on the 20-point circular pattern (Figure 2d). Fast Fourier transform analysis of the fiber distribution confirms an 18° periodicity for the 20-point circles (Figure 2e). In contrast, no periodicity was measured within cells on a dot matrix pattern (Figure 2e).

To determine whether the radial fiber periodicity observed in the cells seeded on the 20-point circle results from cells responding to feature anisotropy or geometric spacing, we generated a hybrid structure that combined the anisotropy of the 20-point circle with the circle dot matrix circle (Figure 2a). After staining for actin, we still observed the formation of strikingly periodic fibers (Figure 2b) and confirmed their periodicity by measuring the angular distribution (Figure 2d). Notably, the periodicity of the actin fibers in cells seeded on the hybrid pattern was weaker than the 20-point circle, likely due to the presence of neighboring features that facilitate redistribution of the actin cytoskeleton. However, this periodicity was significantly higher than that of the dot matrix circle (Figure 2e). This result demonstrates that the cells have preferential sensing of the anisotropic features even in the presence of a more continuous ECM.

Focal Adhesion Distribution on Patterned Surfaces in Response to Anisotropy. Because focal adhesion complexes link the actin cytoskeleton to the ECM, we examined their distribution within cells seeded on anisotropic, periodic, and dot matrix patterns. Immunofluorescence micrographs of vinculin, a focal adhesion protein, show that the focal adhesions primarily form along the periphery of the cell in locations defined by the underlying pattern (Figure 3a-e). Significantly, the focal adhesion geometry reflects the shape of the underlying pattern, and more importantly, the orientation of the actin stress filament is aligned with the fibronectin feature. These results highlight that the geometry and distribution of adhesive cues lead to focal adhesion formation at desired locations with programmed anisotropy, which directs the actin cytoskeletal architecture.

Modulating hMSC Fate in Response to Focal-Adhesion-Defined Actin Arrangements. With the demonstration that anisotropic fibronectin features can direct focal adhesion formation and actin orientation, we investigated whether focal adhesion anisotropy could be used to modulate differentiation independent of cell shape. To evaluate lineage-



Figure 3. Fluorescence micrographs of the focal adhesions and actin cytoskeleton within cells on patterns. (a-e) Representative confocal images of single cells grown on different patterns: square dot matrix (a), anisotropic square (b), dot matrix circles (c), 20-point circles (d), and hybrid circles (e). The nucleus (panel 1), focal adhesions (vinculin, panel 2), and actin cytoskeleton (panel 3) are labeled within each cell. Panel 4 shows the overlay of the different structures.

specific differentiation, we cultured hMSCs on patterns having either anisotropic (anisotropic squares and 20-point circles) or isotropic (square dot matrix and circle dot matrix) ligand arrangements in mixed osteogenic and adipogenic induction media. After 6 days, we fixed and stained cells for osteogenic and adipogenic markers. Cells that stained purple due to alkaline phosphatase activity were counted as osteoblasts, whereas those that stained red from oil droplets (Oil Red O) were counted as adipocytes (Figures 4a and 5a). We also stained the cells with the nuclear dye DAPI and did not score cells that occupied a pattern with a second cell. Color deconvolution was performed on images of single cells to separate and binarize the purple and red channels (Figure S5). The average pixel intensity of each channel was calculated and used to determine if cells were osteogenic or adipogenic (Figures 4b and 5b). Cells with purple channel intensities greater than 2.5 and red channel intensities less than 1.25 were counted as osteogenic, and cells with red channel intensities greater than 1.25 and purple channel intensities less than 2.5 were scored as adipogenic (Figures 4b and 5b). During these experiments, approximately one-half of the cell population differentiated into osteogenic or adipogenic fates (Figure S6).

Cells grown on both square patterns—the square dot matrix and anisotropic—showed a strong preference for osteogenesis over adipogenesis when cultured on larger patterns (54×54 μ m²; Figure 4b,c), as was expected for the strong cue that corners present to a cell and the pro-osteogenic effect of greater spread area.^{23,27} To determine whether focal adhesion anisotropy could synergistically enhance differentiation, we decreased the overall pattern area to reduce the osteogenic cue ($36 \times 36 \ \mu$ m²; Figure 4b,c), and we found a stronger preference for osteogenesis for cells seeded on the anisotropic square patterns compared to those grown on the square dot matrix patterns (Figure 4b,c). These results illustrate how anisotropic arrangements of ligands can synergize with global cell shape to promote an osteogenic fate.

Next, we repeated this experiment for cells cultured on circular patterns. These shapes lack any corners along their perimeter and are known to limit the organization of a contractile cytoskeleton, leading to adipogenic fates.²⁷ As expected, we observed a preference for adipogenesis for cells grown on dot matrix circles (Figure 5b,c). In contrast, cells grown on the 20-point circle patterns preferentially differentiated into osteogenic fates (Figure 5b,c). Significantly, even when cells are grown on the hybrid circle, there is still a



Figure 4. Osteogenic and adipogenic differentiation on square patterns. (a) Bright-field images of cells on each respective pattern strongly staining purple, as an osteogenic marker (left column), or red, as an adipogenic marker (right column). Scale bar: 25μ m. (b) Scatter plots for staining intensity of individual cells after color deconvolution of the red and purple channels from three substrates ($n_{cells} = 759-817$). (c) Percentage of cells staining positive for only adipogenic or osteogenic markers (mean \pm SEM; ***p < 0.001; *p < 0.05; one-way ANOVA with Tukey's honestly significant difference).



Figure 5. Osteogenic and adipogenic differentiation on circular patterns. (a) Bright-field images of cells on each respective pattern strongly staining purple as an osteogenic marker (left column) or red as an adipogenic marker (right column). Scale bar: $25 \ \mu m$. (b) Scatter plots of staining intensity of individual cells after color deconvolution of the red and purple channels from three substrates ($n_{cells} = 263-849$). (c) Percentage of cells staining positive for only adipogenic or osteogenic markers (mean \pm SEM; p = 0.027; one-way ANOVA with Tukey's honestly significant difference *post hoc*).

preference for osteogenic differentiation. For all of our substrates, cells give mixed populations of the two cell fates and, therefore, are not as selective as those in earlier reports that used mechanical stiffness,⁵¹ cell size,²⁷ and cell shape.²³ We expect that future work will demonstrate that the anisotropic subcellular features we show here can be combined with other parameters to synergistically increase yields for the desired cell type. In addition, we examined the nuclear translocation of RUNX2, a primary regulator of osteogenesis, in cells seeded on the circle patterns by examining the nuclear/ cytoplasmic staining intensity. As we found with the alkaline phosphatase stain, cells seeded on the 20-point and hybrid circles showed nuclear staining intensity greater than that of cells seeded on the dot matrix circles (Figure S7). Together, these results demonstrate that the anisotropic fibronectin features, while maintaining a constant shape and size, can redirect cells from primarily adipogenic to osteogenic fates.

Previous work by us and others suggested that the enhanced osteogenesis results from increased contractility of the actomyosin cytoskeleton in the cell.^{23,27,52,53} Therefore, we examined how the anisotropic arrangement of ligands affected the formation of contractile actomyosin fibers (Figure S8). In order to evaluate the actomyosin contractility of hMSCs, we cultured these cells on the square, anisotropic square, circular, and 20-point circle patterns. After 16 h of culture, cells were

fixed and then stained for vinculin, focal adhesions, and myosin IIa. Fluorescent micrographs reveal that myosin IIa is localized along the fibers that have been directed by the anisotropic focal adhesions, suggesting that these user-defined fibers are indeed contractile (for both the square anisotropic and 20-point circle patterns). This observation is especially important for the circular geometry where the 20-point circle drastically alters the contractility by inducing the formation of contractile radial fibers not present in the dot matrix circle. To confirm that myosin IIa plays a significant role in our differentiation on the patterned substrates, we treated cells on the anisotropic square and 20-point circle patterns with blebbistatin, an inhibitor of myosin IIa. In both cases, the cells reversed from an osteogenic fate to an adipogenic fate (Figure S9). Together, these results suggest that the propensity for these cells to differentiate to osteogenic lineages stems from enhanced contractility induced by anisotropic ligand arrangement.

CONCLUSIONS

This work investigates how anisotropic submicron patterns of fibronectin can be used to direct organization of the cytoskeleton. We show that arranging focal adhesions in peripheral areas of cells using nanopatterning enables the controlled reorientation of actin fibers within the interior of cells. The work is also significant because it provides a strategy for modulating actin fiber orientation independently of cell shape, allowing one to confine cells on substrates and program their cytoskeleton. Indeed, our demonstration that hMSCs could be patterned in circular shapes but still undergo osteogenesis reveals the importance of these anisotropic features in directing cell function. The use of PPL to define discrete nanofeatures was critical in this work because it gives the ability to tailor focal adhesion formation over large areas in any arbitrary shape to modulate and study cell behavior. Although a single chemical cue was used in this study, multiplexing with PPL is possible, potentially, allowing one to study the importance of multiple cues in combination with controlled morphology and contractility in influencing cellular fate. This approach to cellular engineering will enable the modulation of cell behavior in complex biological environments, such as those containing multiple different cell types. It creates opportunities for directing stem cells down different lineages within the same confined space to mimic tissue organization. This ability to control and direct cytoskeletal formation can be extended beyond stem cell differentiation to study and control other biological systems such as neurite formation and cancer metastasis.

EXPERIMENTAL METHODS

Substrate Preparation. Glass slides (1.9 cm \times 1.9 cm, 0.5 mm thick, Ted Pella) were sonicated for 30 min, rinsed in ethanol, and dried under a stream of N₂. They were mounted in an electron-beam evaporator (Lesker), and when vacuum reached 2 \times 10⁻⁷ mTorr, 5 nm of Ti and 35 nm of Au were evaporated. Polymer pen arrays having a pen-to-pen distance of 150 μ m were prepared using conventional photolithography techniques according to published methods.⁴² Arrays were coated with an ethanolic solution of 10 mM 16-mercaptohexadecanoic (Sigma) solution for 2 min and dried under N₂. After the Au substrate and pen array were mounted on the PPL system (Tera Fab M Series, Tera Print), the chamber humidity was held at 45% for patterning. Patterns were programmed in the software with tip–substrate dwell times of 2 s. Feature size and quality were confirmed by sacrificing a portion of the substrate, etching Au in the unpatterned areas with a mixed aqueous solution of 13.3 mM

Fe(NO₃)₃ and 10 mM thiourea, and observing the results under an optical microscope. The patterned substrates were then immersed in an ethanolic solution of 10 mM 1-mercapto-11-undecylhexa(ethylene glycol) (Sigma) solution for 1 h to reduce nonspecific protein adsorption. After being rinsed with ethanol and dried with N₂, the substrates were exposed to 50 μ g/mL of human plasma fibronectin (Millipore) in phosphate buffered saline (PBS) and shaken overnight at 4 °C.

Cell Culture. Human MSCs (Lonza) were cultured at 37 °C with 5% CO₂ in basal growth medium supplemented with MSC growth supplements (Invitrogen), L-glutamine (Invitrogen), and gentamycin sulfate amphotericin-1 (5 μ g/mL; Invitrogen). The cells were used between passage 2 and passage 3. For chemical induction of differentiation, cells were cultured in mixed media (1:1 osteogenic/adipogenic induction media, PromoCell; 0.5 μ g/mL, gentamycin). For myosin IIa inhibition studies, 10 μ M of blebbistatin (Stem Cell Technologies) was added to the mixed differentiation media. Approximately 20 000 cells were seeded per substrate. Mycoplasma contamination was monitored using MycoAlertPLUS (Lonza) following the manufacturer's instructions.

Immunofluorescence. hMSCs were cultured on patterned substrates overnight and then fixed in 3.7% paraformaldehyde in PBS for 10 min. After being gently rinsed three times with PBS, cells were permeabilized using 0.3% Triton X-100 in PBS for 1 min and blocked with a 0.1% Triton X-100 in PBS solution with 3% bovine serum albumin for 1 h. For immunofluorescence staining of focal adhesions and actin, primary antibody labeling for vinculin was performed in 1% bovine serum albumin (BSA) in PBS overnight at 4 °C with mouse antivinculin (1:500, Abcam AB18058), followed by secondary antibody labeling using Alexa Fluor 647 labeled goat antimouse (1:250, ThermoFisher A21236) for 1 h at room temperature. Samples were rinsed at least twice with 1× PBS and then actin-labeled using Alexa Fluor 568-labeled phalloidin (ThermoFisher) for 30 min at room temperature. Samples were gently washed three times in PBS and mounted onto glass coverslips using Prolong Gold Antifade reagent with DAPI (ThermoFisher).

For immunofluorescence staining of myosin, samples were incubated in a solution containing an antibody produced in rabbit against nonmuscle myosin IIa conjugated to Alexa Fluor 488 (1:750, Abcam AB204675) and 1% BSA in PBS for 1 h at 4 °C. Vinculin was stained as described above. For RUNX2 staining, hMSCs were prepared for staining as described above. hMSCs were incubated overnight at 4 °C in mouse anti-RUNX2 antibodies conjugated to Alexa Fluor 647 (1:500, Santa Cruz Biotechnology, sc-390351).

Histology. hMSCs were seeded on patterned substrates and cultured for 6 days in the presence of mixed (adipogenic and osteogenic) media. Samples were then rinsed twice with PBS and fixed with 3.7% formaldehyde for 10 min. After being rinsed twice with PBS, samples were permeabilized with a solution of 60% isopropyl alcohol in deionized (DI) H_2O and stained with Oil Red O (Sigma, 60% isopropyl alcohol in DI H_2O) for 30 min at room temperature. Samples were then rinsed once with 60% isopropyl alcohol and then once with PBS and stained for alkaline phosphatase (StemTAG, Cell Biolab, Inc.) for 1 h at room temperature. Samples were rinsed twice with PBS and briefly rinsed in DI H_2O before being mounted onto glass coverslips using Prolong Gold Antifade reagent containing DAPI. All substrates were imaged using a DAPI filter set and phase contrast microscopy using a 10× objective (Zeiss LSM 800).

Microscopy Image Analysis. To generate heatmaps, images of fluorescence images of fixed/stained cells were aligned, stacked, averaged, and pseudocolored to represent regions of high and low density using ImageJ. The orientation of actin fibers in cell micrographs was analyzed using a custom Matlab script that determines orientation using previously reported gradient analysis methods. Briefly, a pixel variance method was used to determine local fiber orientation and magnitude as previously described.⁴⁹ A grayscale threshold, as determined using Otsu's method,⁵⁴ was applied to the gradient images. To eliminate imaging-derived bias from confocal scanning, randomly selected images were rotated along their axis of

symmetry. For square and anisotropic square shaped patterns, fibers were detected within the entire cell as well as those within a region of interest that was drawn to exclude fibers around the edge of the cell. Histograms of pixel orientation were generated for each cell after grouping fiber orientations along mirrored axes (*e.g.*, -45° and $+45^{\circ}$).

For detection of fiber orientation in circular patterns (radial vs circumferential), the center of the cell was detected by fitting a circle around the cells (details for this procedure are included within the Supporting Information) to identify the centroid. The pixel alignment was determined by comparing the detected pixel orientation to the radial coordinates of that pixel relative to the cell centroid. The fibers were classified as either radial ($\pm 30^{\circ}$ from the radial coordinate), or indeterminate (fiber not fitting within the first two groupings). Fast Fourier transform analysis was used to determine the angular periodicity of the fibers within a cell.

Color deconvolution on phase contrast images was performed as previously described²³ using ImageJ (see the Supporting Information). Briefly, the colors were deconvoluted to purple and red channels based upon visual inspection. An intensity cutoff was applied, and the images were binarized (purple and red) to determine cell fate. Cells containing purple were scored as osteocytes, and those with red scored as adipocytes.

Statistical Analysis. All data were analyzed using GraphPad PRISM 5 (GraphPad Software, Inc.). For analysis of fiber orientation, the distribution of orientations was assessed using a two-way ANOVA with Bonferroni *post hoc* analysis. Cell differentiation was assessed using a one-way ANOVA with Tukey's honestly significant difference *post hoc* analysis. Statistical parameters are as follows: Figure 1g ($F_{\text{interaction}} = 18.19, F = 67.65$); Figure 4c (F = 31.37); Figure 5c (F = 7.322).

ASSOCIATED CONTENT

S Supporting Information

The Supporting Information is available free of charge on the ACS Publications website at DOI: 10.1021/acsnano.9b03937.

Information about quantitative methods used to determine fiber orientation and perform color deconvolution, in addition to a general scheme outlining steps to pattern substrates, images showing hMSCs cultured on distinct square and circular patterns, and immunofluorescence images of cells stained for RUNX2, myosin IIa, and vinculin (PDF)

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Notes

The authors declare no competing financial interest.

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